



2013.10.24, TUM-IAS, Garching bei München

# X-ray Phase-contrast CT with lab-based X-ray sources

**Martin Bech**

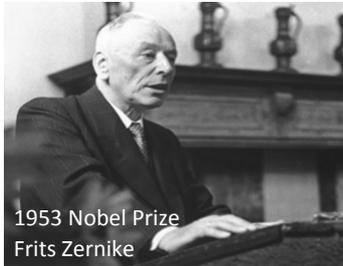
Technical University Munich (TUM) and  
Medical Radiation Physics, Lund University

## Outline



- what is x-ray phase-contrast and dark-field imaging?
- synchrotron radiation setup – coherent beam
- laboratory setup – incoherent beam

## Visible light: Several contrast modalities



1953 Nobel Prize  
Frits Zernike



Zeiss  
microscope  
[www.zeiss.de](http://www.zeiss.de)

fibroblast cells



bright-field  
contrast



phase-contrast  
(DIC)



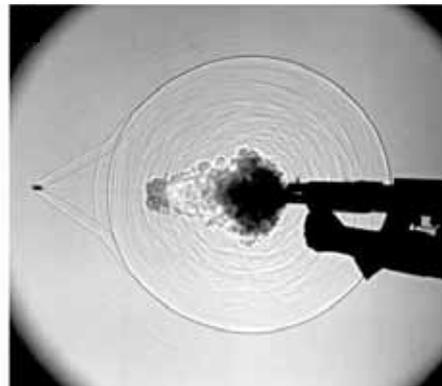
dark-field  
contrast

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## Visible light phase contrast



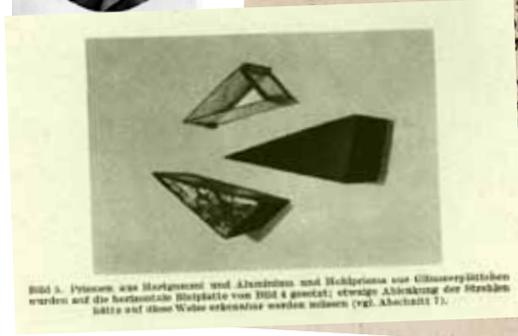
Shadowgraph



Wikipedia: (images by Gary S. Settles, Penn State Gas Dynamics Lab)

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# Röntgen was also looking for refraction...



# Wave propagation for pedestrians

Wave propagation regimes: Fresnel number:  $F = \frac{a^2}{\lambda Z}$

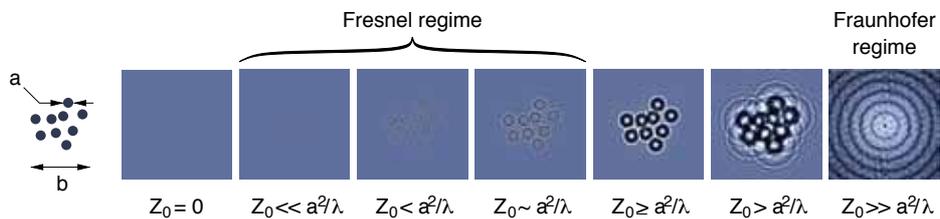


Figure courtesy: Timm Weitkamp, Phil Willmott



### X-ray tube and 2D detector

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*M. Hobeisel / Nuclear Instruments and Methods in Physics Research A 563 (2006) 215–224*



Fig. 1. (a) Ms. Röntgen's hand with ring (first X-ray image taken on December 22, 1895), (b) an early radiological workplace where the patient had to hold the film cassette himself, and (c) fluoroscopy in the Gynaecological Hospital, Erlangen (1918).



## Synchrotron radiation

# Holography



5010

F van der Veen and F Pfeiffer

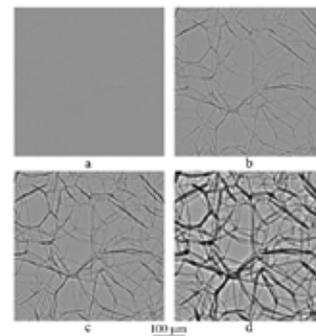
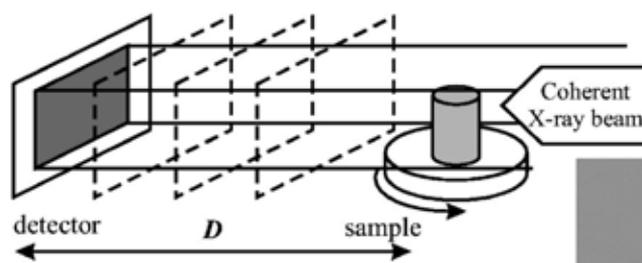


(a) distance: 0 mm



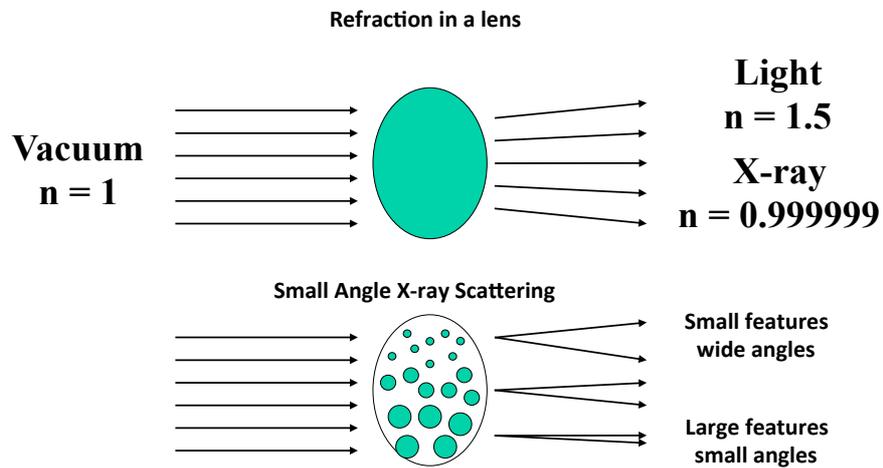
(b) distance: 100 mm

# Holotomography



Polystyrene foam.  
P. Cloetens 1999

## Refraction and scattering



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## History of phase contrast imaging

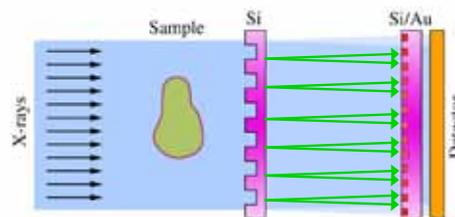


Grating Interferometer:

Synchrotron  
David 2002, Momose 2003  
Weitkamp 2005

X-ray tube  
Pfeiffer 2006

Darkfield  
Pfeiffer 2008



A. Momose et al., *Jpn. J. Appl. Phys.* **42** L866 (2003)  
T. Weitkamp et al., *Optics Express* **13**, 6296 (2005)  
F. Pfeiffer et al., *Nature Physics* **2**, 258 (2006)  
F. Pfeiffer et al., *Nature Materials* **7**, 134-137 (2008)

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## Three signals for imaging



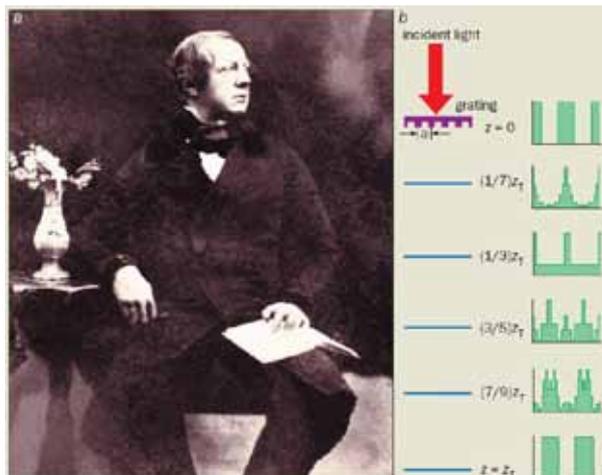
- Absorption – Standard x-ray image
- Refraction – Phase-contrast image
- Scattering – Dark-field image

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## Talbot Effect

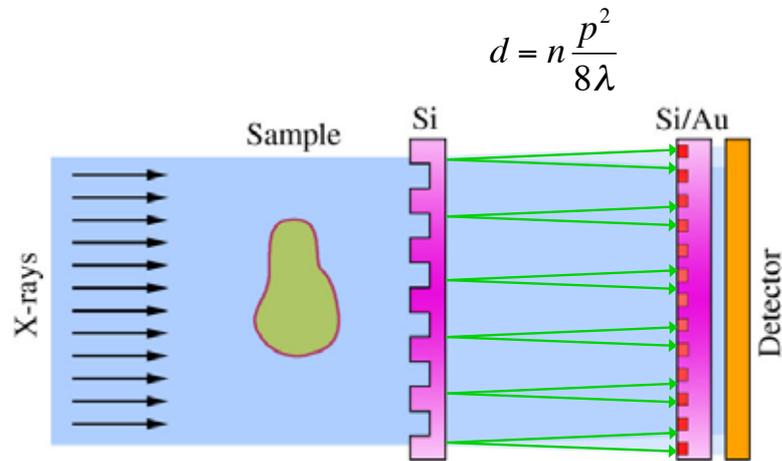


1800 - 1877



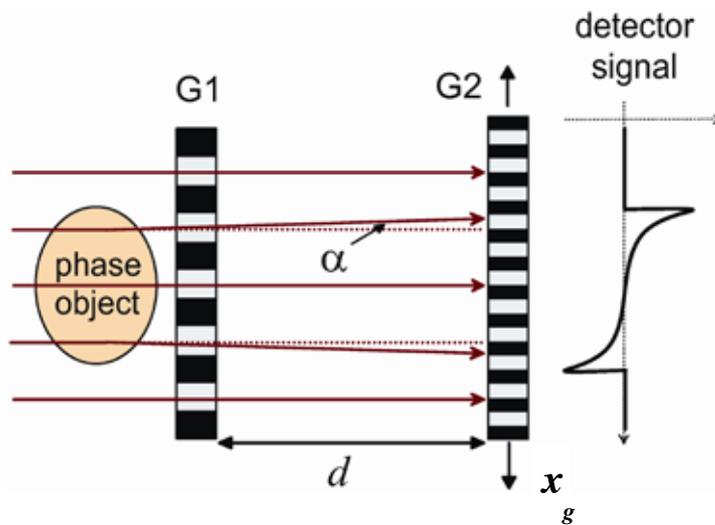
Sir Henry Fox Talbot 1836

## Talbot self imaging

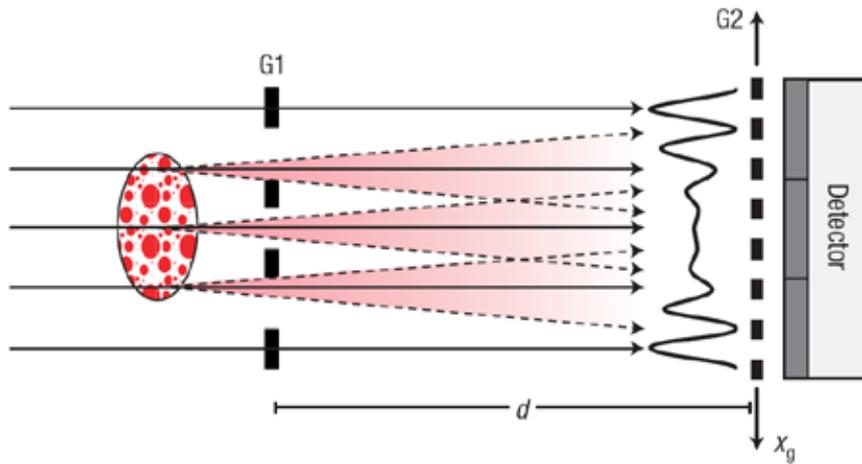


T. Weitkamp et al., Optics Express 13, 6296 (2005)  
F. Pfeiffer et al., Nature Physics 2, 258 (2006)

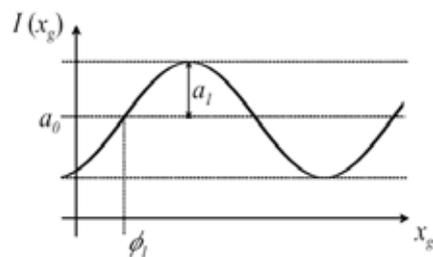
## Differential Phase Imaging



# Scattering



# Extracting phase contrast image



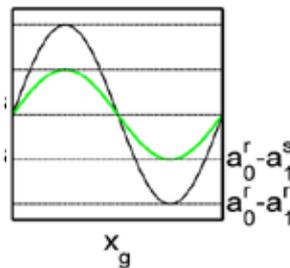
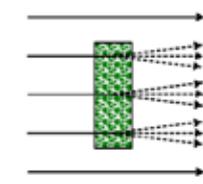
$$I(m, n, x_g) = \sum a_i(m, n) \cos(ikx_g + \phi_i(m, n))$$

$$\approx a_0(m, n) + a_1(m, n) \cos(kx_g + \phi_1(m, n))$$

absorption

local scattering power !

phase gradient

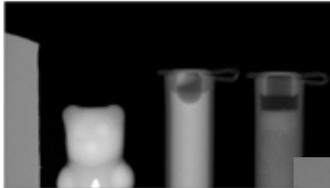


F. Pfeiffer et al., Nature Materials 7, 134-137 (2008)

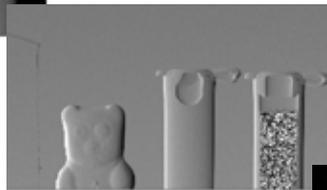
## Three signals for imaging



Absorption – Standard x-ray image



Refraction – Phase-contrast image



Scattering – Dark-field image



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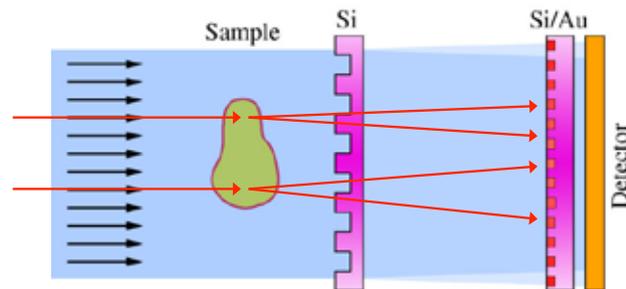
## New material parameter: Linear diffusion coefficient



$$A(x) = \frac{1}{\sigma d \sqrt{2\pi}} \exp\left(-\frac{x^2}{2\sigma^2 d^2}\right)$$

$$I^s(x) = I^r(x) \otimes A(x)$$

$$V \equiv \frac{V^s}{V^r} = \exp\left(\frac{-2\pi^2}{p^2} \sigma^2 d^2\right)$$



$$\sigma^2 = \int \epsilon(y) dy$$

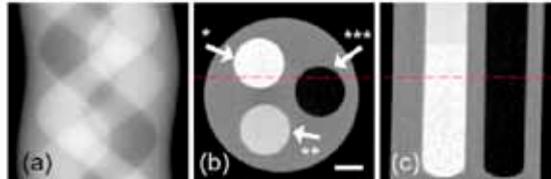
$$V(x) = \exp\left(\frac{-2\pi^2 d^2}{p^2} \int \epsilon(x, y) dy\right)$$

M. Bech et al, Phys. Med. Biol. 55, 5529 (2010)

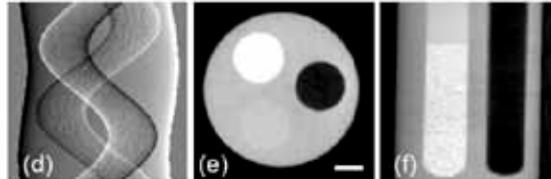
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## From 2D to 3D: Quantitative Phase-Contrast CT

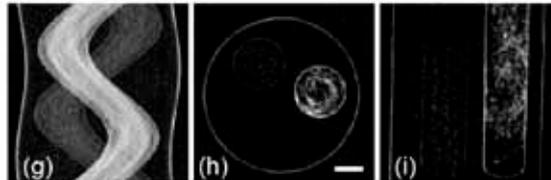
Attenuation CT



Phase CT



Darkfield CT



Bech et al  
PMB | 2010



# Synchrotron radiation

## At the Synchrotron Radiation Source



- Two gratings
- Holography / Holo-tomography possible
- Synchrotron radiation source
- Pros:
  - High Brilliance (high flux in narrow band)
  - Good coherence
- Cons:
  - Limited access
  - Limited field of view

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## ESRF ID-19

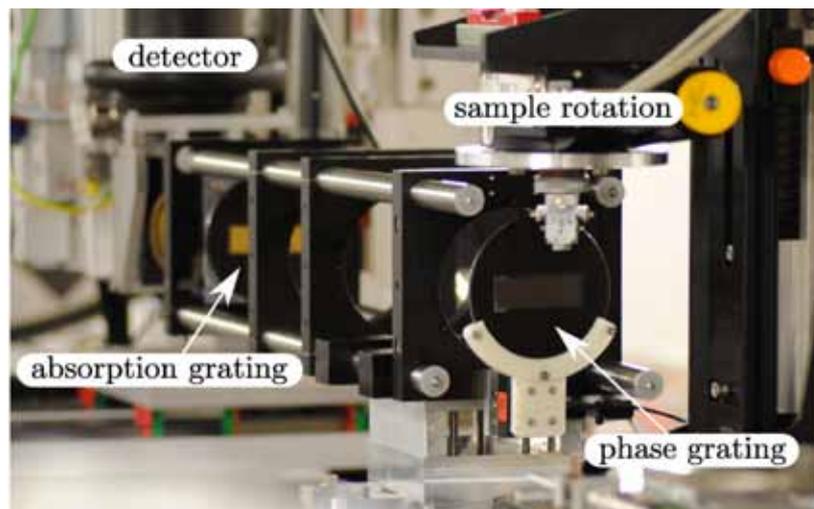
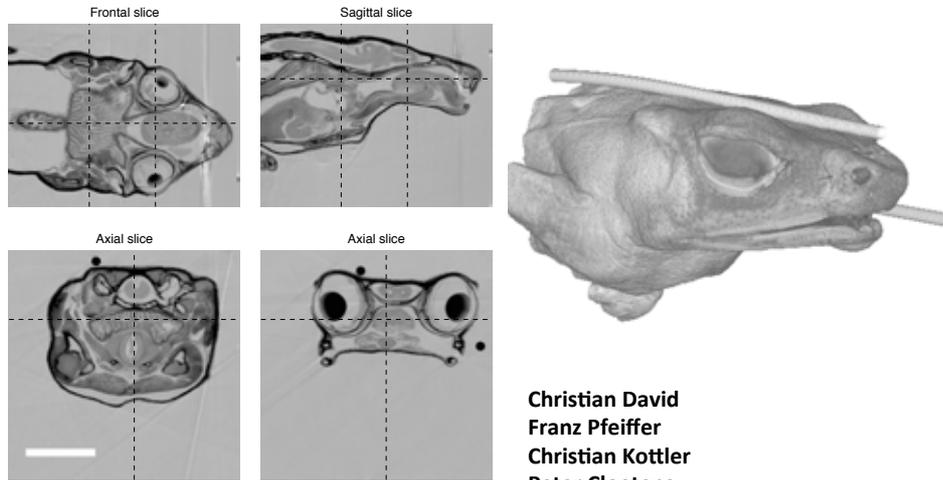
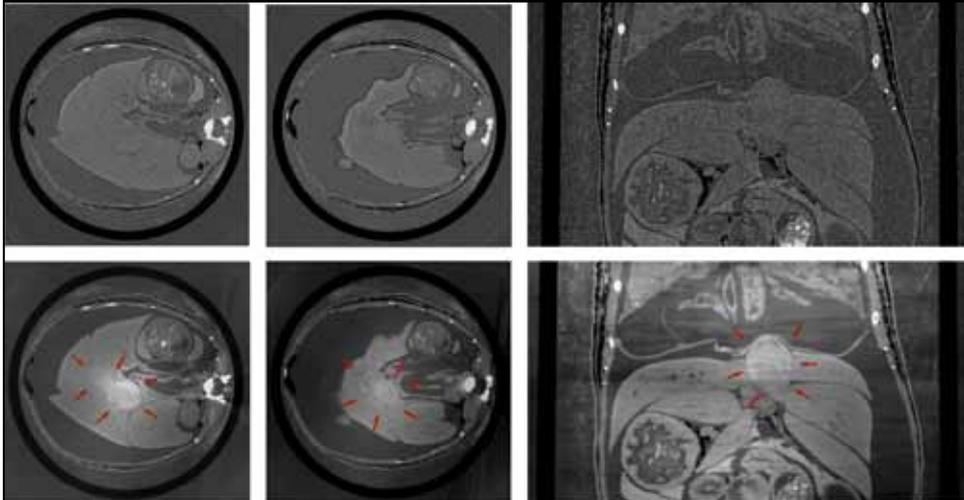


Figure courtesy: Irene Zanette, Arne Tapfer



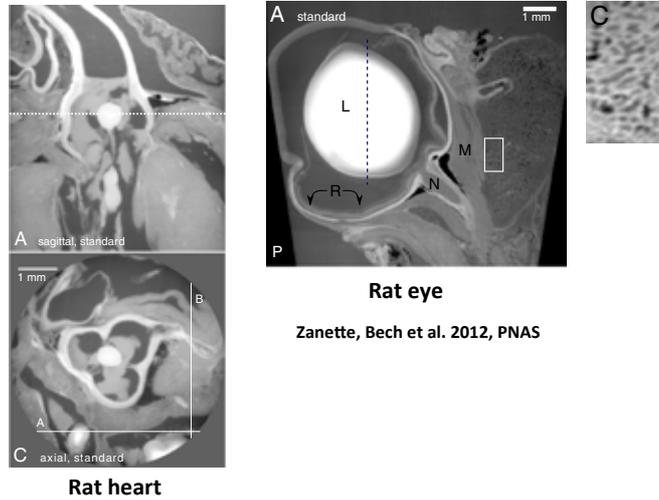
conventional  
microCT



2010

phase-contrast  
microCT

## High resolution soft tissue imaging



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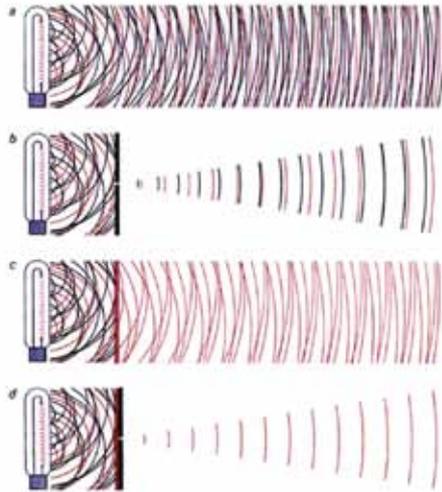
## In the Laboratory



- Three gratings
- Traditional x-ray tube source
- Pros:
  - Large field of view
  - Cheap
  - Convenient
- Cons:
  - Low flux
  - Polychromatic
  - Poor coherence

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# Coherence



Courtesy of A. Schawlow, Stanford

# Three Grating principle

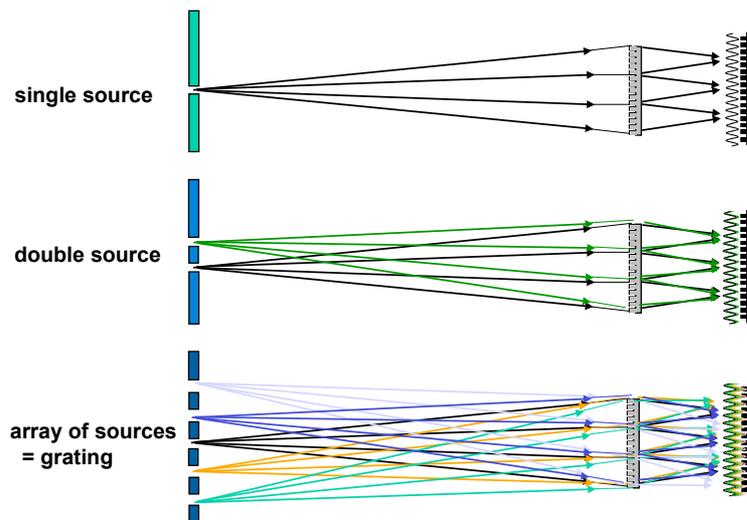
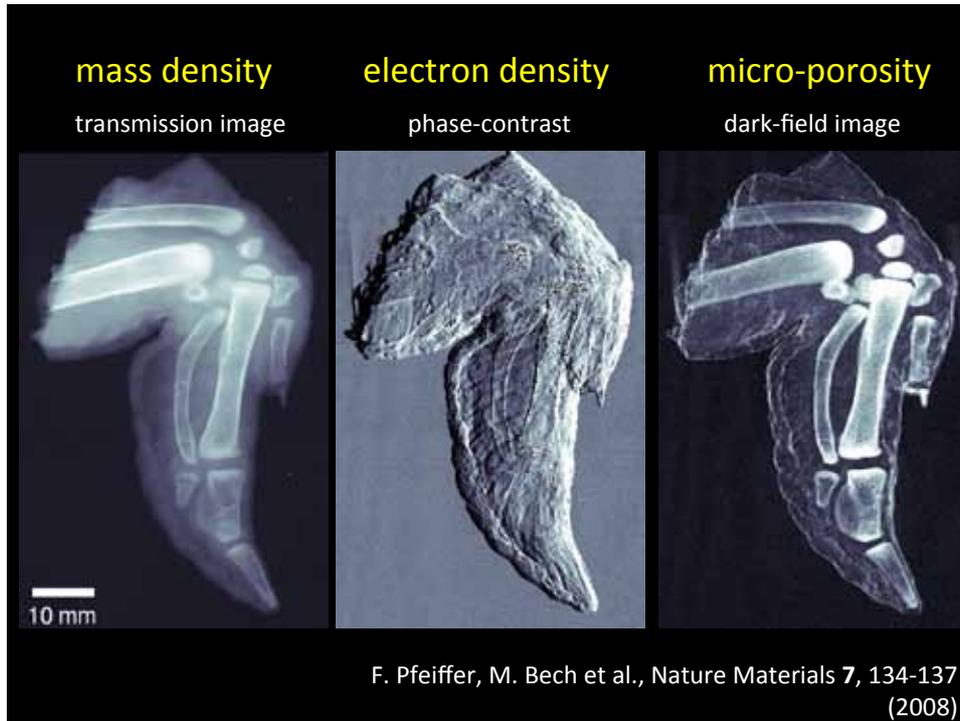


Figure courtesy: C. David, PSI



**Phase Contrast micro-CT**



**SKYSCAN**  
now Bruker  $\mu$ CT

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## Requirements for in-vivo experiments



- Rotating gantry around small animal
  - Stable both in rotation as for the alignment of the gratings
  - Compact design
- Acceptable radiation dose for repetitive studies
- Fast – to limit time of anesthesia of the animal

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## Skyscan 1190, GBI phase-contrast scanner



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# 1190 phase scanner gantry



## Setup in Rotating Gantry

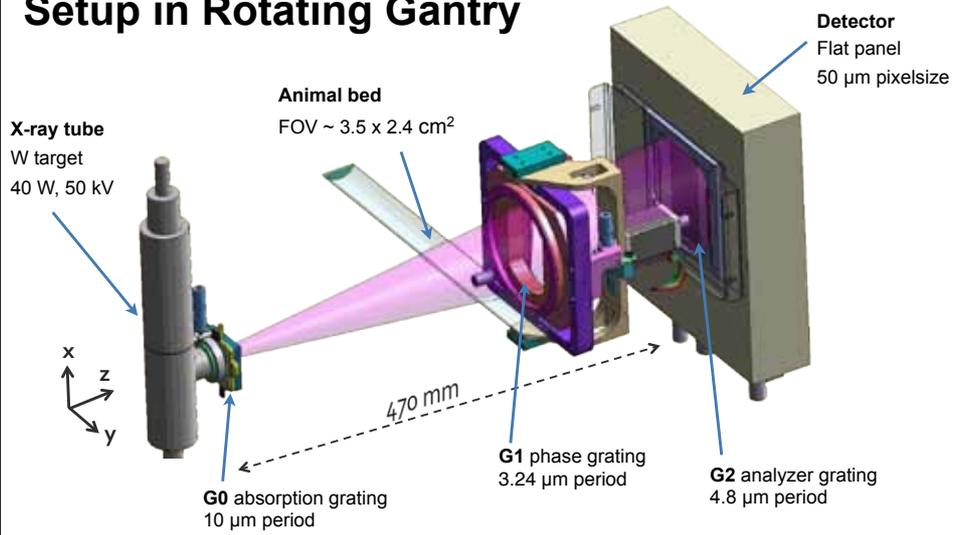


Image courtesy: Bart Pawels, Skyscan

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## Complementarity of information

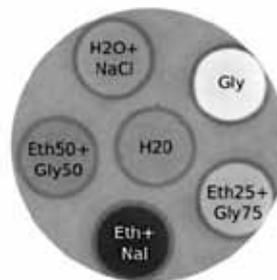


**'conventional'**  
Hounsfield Units



$$\frac{\mu - \mu_{\text{water}}}{\mu_{\text{water}} - \mu_{\text{air}}}$$

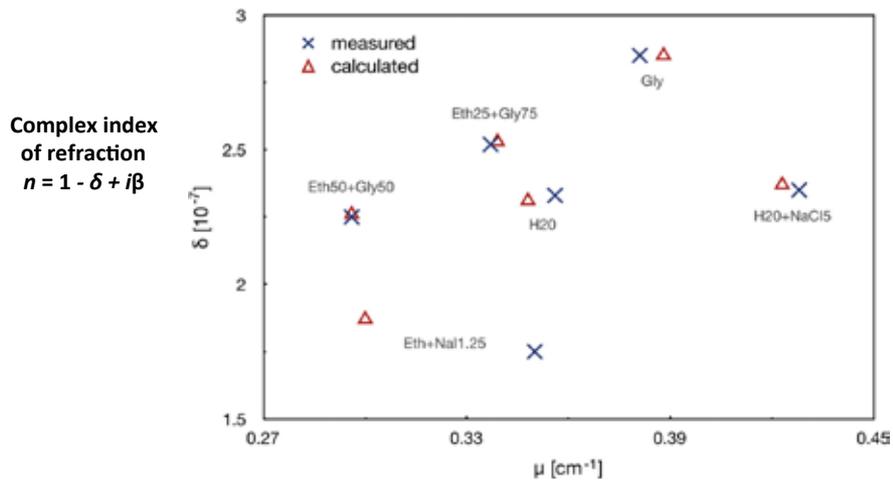
**'phase-contrast'**  
Hounsfield Units



$$\frac{\delta - \delta_{\text{water}}}{\delta_{\text{water}} - \delta_{\text{air}}}$$

Tapfer et al | Med Phys | 2011 & Tapfer et al | PNAS | 2012

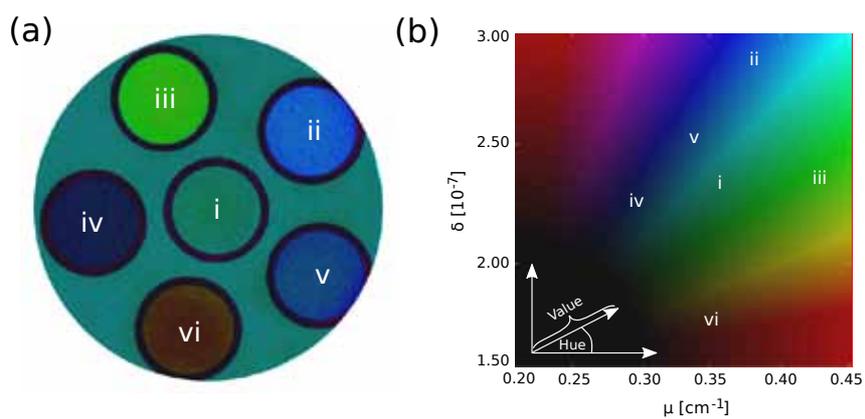
## Quantitative results



A. Tapfer *et al.*, Medical Physics 38 (11) 2011, 5910-5915

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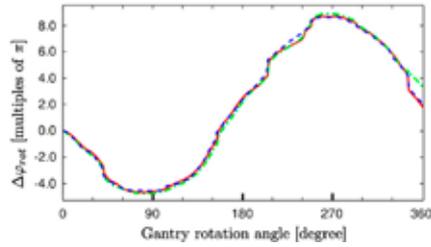
## Quantitative results



A. Tapfer *et al.*, Medical Physics 38 (11) 2011, 5910-5915

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## Effect of gantry rotation on phase stability



Measured interferometer phase shift upon gantry rotation (3x)

uncorrected projection

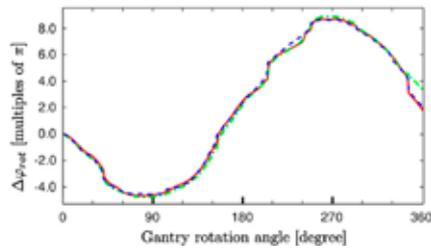
phase ramp

corrected image



Tapfer et al | PNAS | 2012

## Effect of gantry rotation on phase stability



Measured interferometer phase shift upon gantry rotation (3x)

uncorrected projection

phase ramp

corrected image

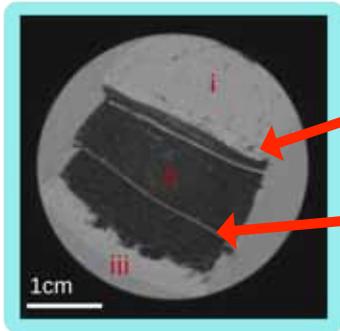


Tapfer et al | PNAS | 2012

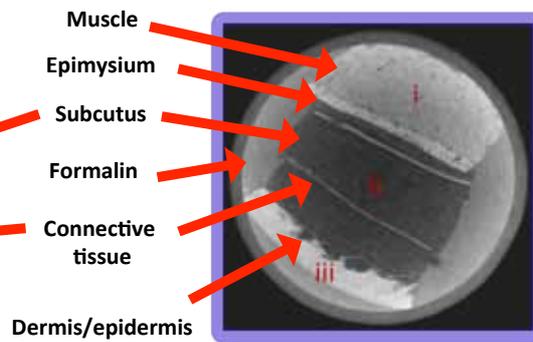
## Formalin fixated porc



Attenuation image



Phase image



Muscle  
Epimysium  
Subcutus  
Formalin  
Connective tissue  
Dermis/epidermis

40 kV/750  $\mu$ A  
rot. step of 0.24°  
8 phasesteps

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## Medical imaging



### *Mouse, in-vivo*

A Dark-field



B Attenuation



C Phase-contrast



Bech et al. Scientific Reports, accepted 2013



## Dark-field imaging for lung emphysema diagnostics

**S. Schleede, A. Yaroshenko, A. Malecki, M. Bech, J. Herzen, K. Achterhold, F. Pfeiffer**  
*Technical University Munich, Germany*

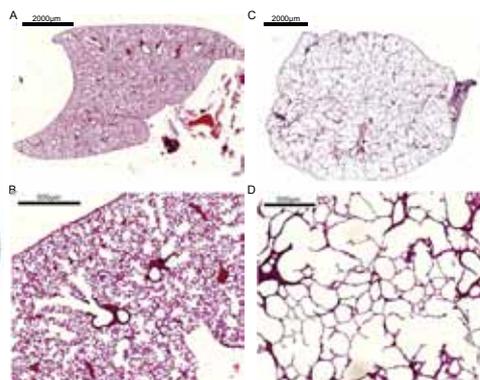
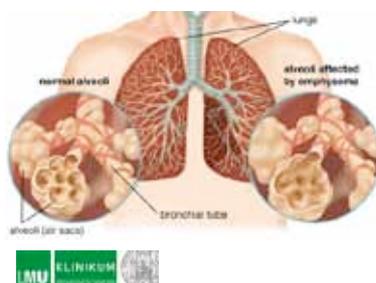
**F. Meinel, S. Adam-Neumaird, S. Thieme, F. Bamberg, K. Nikolaou, M. Reiser**  
*Radiology Department, Ludwig Maximilians University Munich, Germany*

**A.Ö. Yildirim, A. Bohle, O. Eickelberg**  
*Helmholtz Center for Health, Munich, Germany*

## Lung imaging



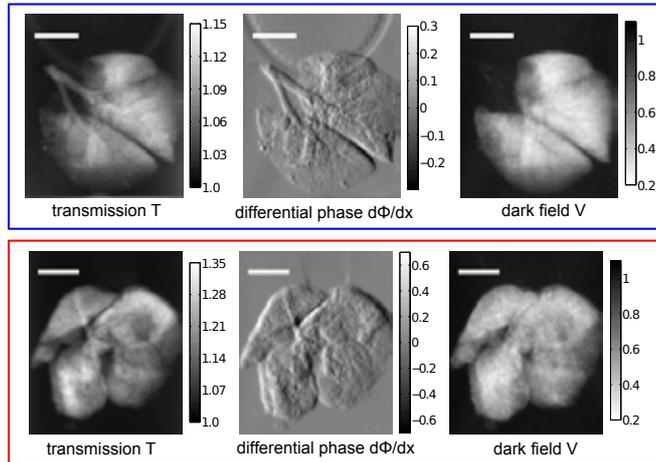
### Chronic Obstructive Pulmonary Disease (COPD)



pulmonary emphysema: mouse model



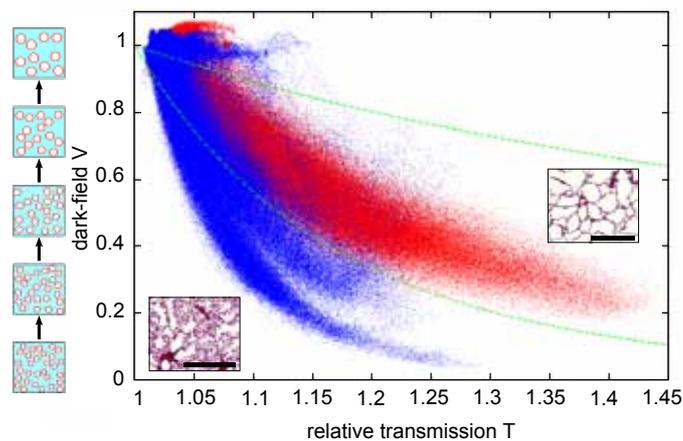
*Emphysema lung, Synchrotron radiation*



Schleede, Meinel, Bech et al. 2012. PNAS



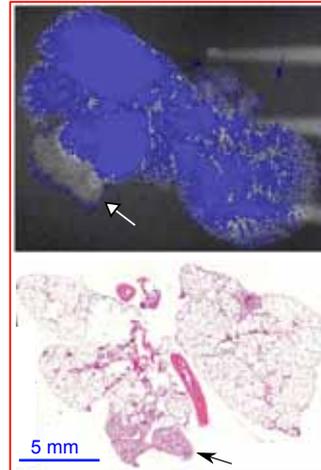
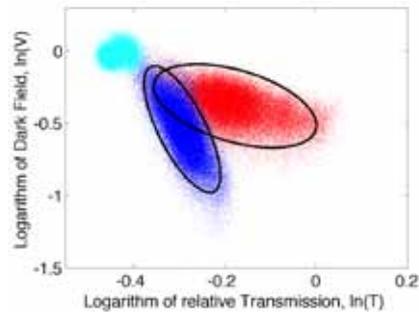
*Emphysema lung, Synchrotron radiation*



Schleede, Meinel, Bech et al. 2012. PNAS



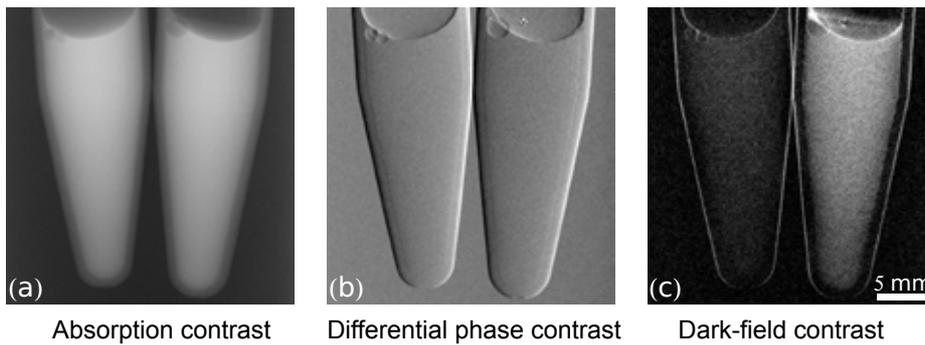
*Emphysema lung, X-ray tube*



Yaroshenko, Meinel, Bech et al. Radiology 2013



Optison microbubbles



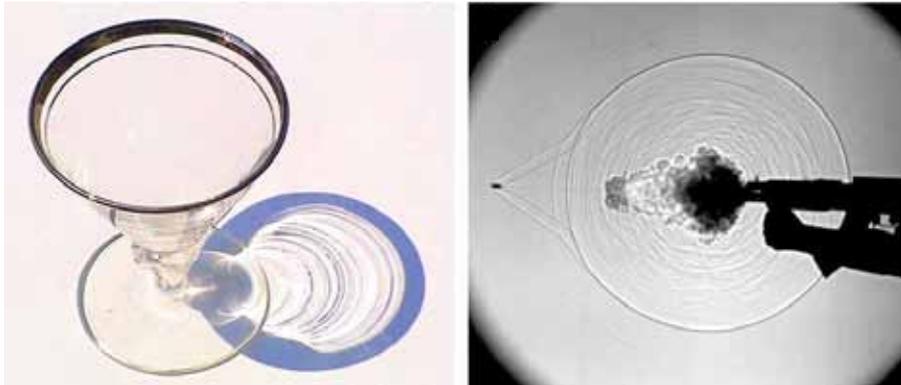
Scan parameters: 30 kVp, 10 phase steps, 10 sec exposure time

Velroyen, Bech et al. Physics in Medicine and Biology 2013

## Thank you for your attention



### Shadowgraph



Wikipedia: (images by Gary S. Settles, Penn State Gas Dynamics Lab)

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## Acknowledgement



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Skyscan / Bruker  $\mu$ CT



Felix Meinel, Fabian Bamberg, Konstantin Nikolaou, Max Reiser  
Klinikum Grosshadern, Munich